

Cholesterol Penetration into Daily Disposable Contact Lenses Using a Novel *In Vitro* Eye-Blink Model

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Introduction

- Daily disposable (DD) lens materials continue to show an increase in use for practitioners and patients and provide lens wearers with a decreased proportion of complications, improved comfort and visual acuity, and lower quantities of lens deposits.¹⁻⁸
- Lipid uptake on silicone hydrogel (SH) DDs is far less than on their daily wear material counterparts.^{9, 10}
- However, current *in vitro* methods/models to evaluate tear film (TF) deposition on various contact lens (CL) materials do not simulate physiological eye conditions, such as tear flow or blink motion.^{9, 11-15}
- Several unique *in vitro* eye models have been developed to include tear flow or tear replenishment,^{16,17} intermittent air exposure,¹⁸ or *in vivo* fouling,¹⁹ generating results differing from those obtained with the static vial model.

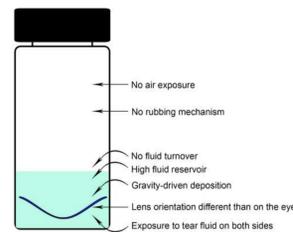


Figure 1. Drawbacks of using a simple vial model to evaluate contact lenses

Purpose

- To determine differences in lipid uptake penetration, comparing a traditional static incubation method with a novel *in vitro* eye model.

Materials & Methods

- Three silicone hydrogel (SH) and four conventional hydrogel (CH) DD were tested:
 - ❖ Delefilcon A (Dailies Total1®; Alcon)
 - ❖ Somofilcon A (clariti® 1day; CooperVision)
 - ❖ Narafilecon A (1-Day Acuvue® TruEye®; Johnson & Johnson)
 - ❖ Etafilecon A (1-Day Acuvue® Moist®; Johnson & Johnson)
 - ❖ Ocufilecon B (Biomedics® 1day, CooperVision)
 - ❖ Nesofilecon A (Biotrue® ONEday; Bausch + Lomb)
 - ❖ Nelfilcon A (Dailies® AquaComfort Plus®, Alcon)
- CLs were incubated for 4 hours (h) and 12 h in an artificial tear solution (ATS) containing a variety of proteins and lipids (mucin, albumin, lysozyme, triolein, cholesterol ester, cholesteryl oleate, phosphatidylcholine, oleic acid methyl ester).
- In addition, a small amount of cholesterol, labeled with 7-nitrobenz-2-oxa-1,3-diazol-4-yl (NBD) fluorophore, was added to the ATS.
- Contact lenses (n=3) were incubated at room temperature (21°C), employing two different methods:
 - ❖ in a vial containing 3.5 mL of ATS on a orbital shaker, and
 - ❖ using our novel *in vitro* eye-blink model (OcuFlow), which consist of a “corneal/scleral eye piece” and a “eyelid piece” that are attached to two individual actuators, which enable us to simulate a blinking motion. Furthermore, through a microfluidic pump, we simulated a physiological tear flow of 1.3µL/min.

Materials & Methods cont'd

- After incubation, the central and peripheral 5 mm of each CL were punched out and mounted on a microscope slide.
- Subsequently, the penetration of NBD-cholesterol within the lens materials was determined by laser scanning confocal microscopy (LCMS) with argon laser at 488 nm.
- CLs were optically sectioned at 0.5 µm intervals (z stack).
- The fluorescence intensity profile of each CL sample was calculated with ImageJ software, using the “Plot Z axis profile” module.
- Curves of relative intensity of fluorescence (RIF) were plotted using Graphpad Prism

Results

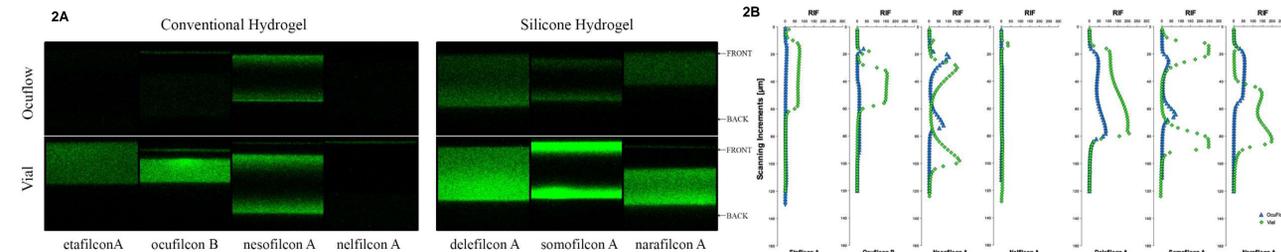


Figure 2. A) Composite representative confocal image illustrating the lipid distribution in the central section of various CLs after 4 h incubation with NBD-cholesterol in the vial as compared to the eye model; B) RIF across the thickness of the CL samples in the vial as compared to the eye model

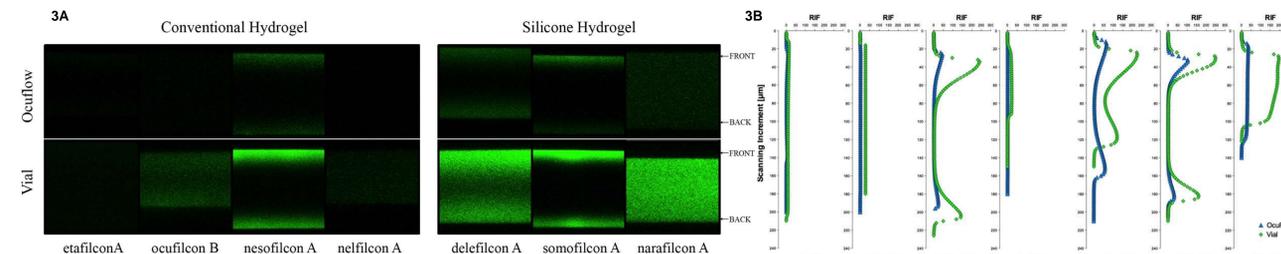


Figure 3. A) Composite representative confocal image illustrating the lipid distribution in a peripheral section various CLs after 4 h incubation with NBD-cholesterol in the vial as compared to the eye model; B) RIF across the thickness of the CL samples in the vial as compared to the eye model

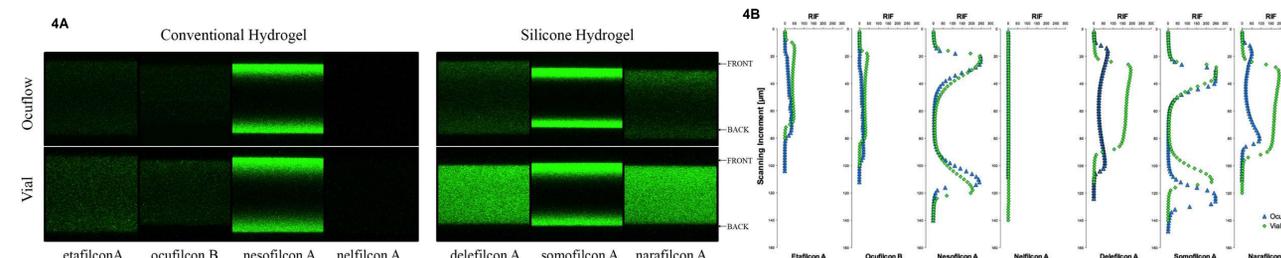


Figure 4. A) Composite representative confocal image illustrating the lipid distribution in the central section of various CLs after 12 h incubation with NBD-cholesterol in the vial as compared to the eye model; B) RIF across the thickness of the CL samples in the vial as compared to the eye model

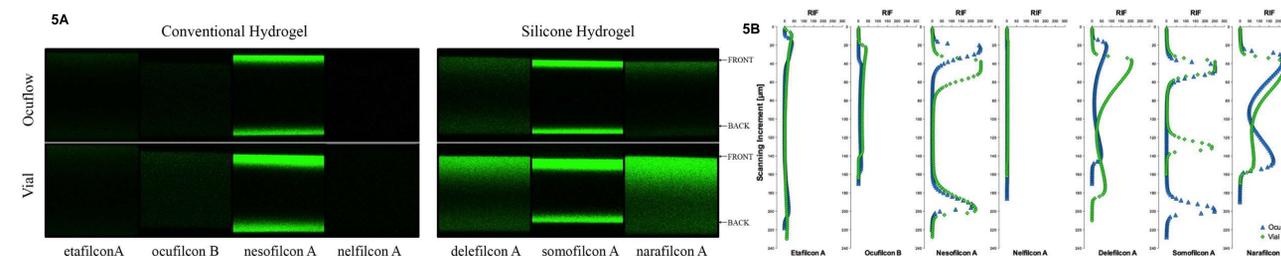


Figure 5. A) Composite representative confocal image illustrating the lipid distribution in a peripheral section of various CLs after 12 h incubation with NBD-cholesterol in the vial as compared to the eye model; B) RIF across the thickness of the CL samples in the vial as compared to the eye model

Results cont'd

- Penetration profiles of the TF lipid vary between the static and the eye-blink (OcuFlow) model incubation methods.
- Incubating the lenses traditionally (in a vial) showed lipid uptake throughout the lens material, starting from both sides of the contact lenses.
- However, employing our eye-model (OcuFlow), cholesterol penetration was less and can be seen starting from the front surface of the lenses.
- SHs showed higher RIF than CH lens materials, except for nesofilecon A.
- Furthermore, RIF varied between incubation methods, incubation time, lens materials, and between the centre and periphery of the lens materials, with the traditional method showing more RIF than our novel eye-model (OcuFlow).

Conclusions

- The results of this study provide new insight and a novel *in vitro* approach on the penetration of tear film components on/into contact lenses.
- Furthermore, we can show that the traditional methods used for *in vitro* lens incubation expose the materials to amounts of ATS that exceed physiological limits, which can lead to overestimating lipid deposition.
- This novel eye-blink platform (OcuFlow) is able to better simulate on-eye conditions than previous models and will help to further our knowledge about the interactions between CLs and TF components, *in vitro*.

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Acknowledgements



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